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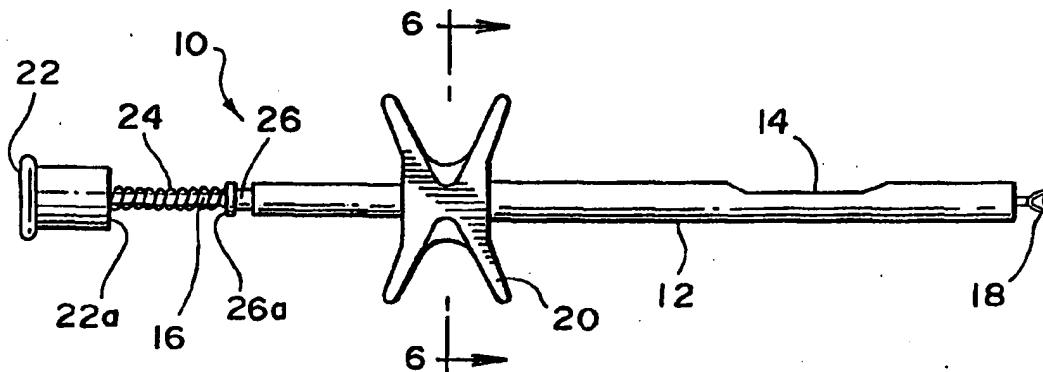
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(54) Title: INJECTION SYSTEM AND METHOD FOR USE WITH A DEFORMABLE INTRAOCULAR LENS



(57) Abstract

This invention is a lens injecting device (10) including a slidable plunger (16) and means for providing a force (24) in a direction opposite to the direction of advancement of the slidable plunger (16) to provide controlled release of the deformable intraocular lens from the lens injection device (10). Further this is a method of implantation of a deformable intraocular lens in the eye by forcing the deformable intraocular lens in a folded or condensed configuration through a passageway through an incision in the eye while applying an opposing force to control release of the deformable intraocular lens into the eye.

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Title of the Invention

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INJECTION SYSTEM AND METHOD FOR USE WITH A DEFORMABLE INTRAOCULAR LENS***Related Applications***

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This is a continuation-in-part application of U.S. Patent Application entitled "DEFORMABLE INTRAOCULAR LENS CARTRIDGE", Serial No. 08/197,604, filed on February 17, 1994, and U.S. Patent Application entitled "DEFORMABLE INTRAOCULAR LENS INSERTION SYSTEM", Serial No. 08/221,013, both fully incorporated by reference herein.

15

Field of the Invention

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This invention is directed to a deformable intraocular lens injecting system for surgical implantation of a deformable intraocular lens in the eye. The deformable intraocular lens injecting system preferably comprises a lens injecting device and a lens cartridge. This invention also is directed to a method of using the deformable intraocular lens injecting device according to the present invention, and a method of inserting the deformable intraocular lens into the eye.

Background of the Invention

Presently, deformable intraocular lens are being surgically implanted by various techniques. The majority of these surgical procedures in the United States and abroad involve
5 the use of either 1) surgical forceps; or 2) "shooter" devices for mechanically deforming (e.g., folding, compressing, condensing, rolling, etc.) and manipulating the deformable intraocular lens in a manner to allow insertion through a small incision (2.5 to 3.0 mm) in the eye.

STAAR Surgical Company of Monrovia, California, the inventors and originators of the
10 deformable intraocular lens with Dr. Mozzocco, have also been the innovators and suppliers of "shooter" devices to the industry. These "shooter" devices have been widely accepted and currently used by surgeons specializing in the implantation of deformable intraocular lenses.

STAAR Surgical Company informally estimates that approximately fifty (50) percent of
15 all surgical procedures involving the implantation of deformable intraocular lens occur with the use of "shooter" devices.

The original "shooter" devices proposed and designed by Dr. Mozzocco were configured
20 to directly receive a loose unprotected deformable intraocular lens. In such devices, the fully exposed deformable intraocular lens could be potentially damaged while loading the "shooter"

device with the deformable intraocular lens. In further developing "shooter" type devices, STAAR Surgical Company made the first "shooter" system comprising an injecting device and a separate one-piece foldable lens cartridge having a lens holding portion connected to a nozzle portion. This development resulted in a "shooter" device that became known in the industry as
5 the "STAAR Shooter". The "STAAR Shooter" became available around 1986, and was supplied on an experimental use basis to surgeons participating in clinical studies seeking approval of implantation of deformable intraocular lens in the human eye by the Food and Drug Administration (FDA), which approval occurred in 1991. An example of a prior art shooter device of STAAR Surgical Company is shown in Figures 12 and 13.

10

The prior art shooter device shown in Figures 12 and 13 includes a freely slideable plunger that can be advanced by simply pushing on the one end of the plunger. The slideable plunger includes a tip for contacting with the deformable intraocular lens loaded in a foldable type lens cartridge and forcing the deformable intraocular lens through a nozzle portion of the
15 lens cartridge inserted through a small incision in the eye.

The standard method of use of the prior art shooter device comprises the steps of:

- 1) loading a deformable intraocular lens into an foldable type lens cartridge opened
20 for receiving the deformable intraocular lens in a flat configuration;

- 4 -

2) closing the foldable type lens cartridge which causes the deformable intraocular lens to fold inside the passageway through the lens cartridge;

3) inserting the loaded lens cartridge into the "STAAR Shooter" device;

5

4) inserting the tip of the nozzle portion of the lens cartridge through the incision into the eye;

10 5) advancing the plunger by pushing on the end of the plunger with the thumb while gripping the finger grip connected to the barrel with index finger above and middle finger below so that the tip of the plunger enters into the end of the passageway through the lens cartridge, and then contacts with a trailing end of the deformable intraocular lens; and

15 6) further advancing the plunger by further pushing on the end of the plunger so that the plunger tip forces the deformable intraocular lens through the passageway in the lens cartridge and out through a tip of the nozzle portion extending through the incision in the eye, thus, allowing the unconstrained deformable intraocular lens to open up (i.e. unfold or decompress) inside the eye.

- 5 -

The manner in which the deformable intraocular lens is released from the tip of the nozzle portion inside the eye can be an important factor with respect to the degree of success of the surgical procedure, and risk of harm or damage to eye tissue during the surgical procedure. In order to increase the degree of success of the surgical procedure and minimize
5 the risk to the patient, it is highly desirable that the deformable intraocular lens is released in a controlled manner, since uncontrolled release of the deformable intraocular lens could cause eye damage. Specifically, due to the resilient nature of the plastic material of the deformable intraocular lens and the plastic material of the nozzle portion of the lens cartridge, the deformable intraocular lens has a tendency to shoot out of the end of the tip of the nozzle portion
10 when uncontrollably released. This phenomenon occurs due to the highly compressed or constrained (i.e. "stressed") configuration of the deformed intraocular lens attempting to expand inside the nozzle portion having resilient walls. When a certain portion of the deformable intraocular lens is extruded or projected a certain critical distance outside the opening of the tip of the nozzle portion, the "stressed" lens will tend to suddenly release and shoot out of the tip of the nozzle portion into the interior of the eye. This phenomenon can result in torn capsular
15 bags and/or damage to tissue in the anterior and posterior chambers in some cases.

In order to control the release of the intraocular lens, various known modifications to the shooters and lens cartridges have been made, and insertion techniques have also been modified.
20 For example, the tip of the nozzle portion can be provided with slits that control the opening and

- 6 -

alleviate the expansion force of the folded or compressed intraocular lens exiting the tip of the nozzle portion. Further, the plunger in some shooters is not freely slideable, but instead provided with threaded means for advancing the movement of the plunger. For example, STAAR Surgical Company currently provides a "shooter" under the Model No. MSI-T having a plunger
5 with threaded advancement means allowing for highly controlled fine advancement of the plunger, which provides some controlled release of the deformable intraocular lens.

However, this type of "shooter" having threaded advancing means for controlling the movement of the plunger is not considered desirable by some high volume and high skilled
10 surgeons performing multiple surgical procedures one after another, since any means for restricting the movement of the plunger impedes the surgeon increasing the time for each procedure and potentially limits the maneuverability of the "shooter".

Thus, it is highly desirable to improve both the devices and methods of implanting the
15 deformable intraocular lens in the eye to provide controlled release of the deformable intraocular lens into the eye, and for decreasing the time of the surgical procedure. Also, the ergonomic "feel" for the surgeon using the "shooter" devices can be enhanced by "shooters" according to the present invention tending to increase surgical efficiency and decrease the risk to the patient.

Summary of the Invention

A first object of the present invention is to provide a deformable intraocular lens injecting system providing controlled release of the deformable intraocular lens into the eye.

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A second object of the present invention is to provide a deformable intraocular lens injecting system having means for controlling the release of the deformable intraocular lens into the eye.

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A third object of the present invention is to provide a deformable intraocular lens injecting system comprising a nozzle portion having means for controlling the release of the deformable intraocular lens into the eye.

15

A fourth object of the present invention is to provide a deformable intraocular lens injecting system comprising a lens cartridge having a nozzle portion with means for controlling the release of the deformable intraocular lens into the eye.

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A fifth object of the present invention is to provide a deformable intraocular lens injecting system comprising a lens cartridge having a nozzle portion with one or more frangible walls or wall portions for controlling the release of the deformable intraocular lens into the eye.

- 8 -

A sixth object of the present invention is to provide a deformable intraocular lens injecting system comprising a lens injecting device having a movable plunger with means for controlling the release of the deformable intraocular lens into the eye.

5 A seventh object of the present invention is to provide a deformable intraocular lens injecting system comprising a lens injecting device having a plunger with a spring to control the movement of the plunger and in effect control the release of the deformable intraocular lens into the eye.

10 An eighth object of the present invention is to provide a deformable intraocular lens injecting system comprising a lens injecting device having a slidable plunger with a spring to control an end portion of the movement of the plunger and in effect control the release of the deformable intraocular lens into the eye.

15 A ninth object of the present invention is to provide a deformable intraocular lens injecting system comprising a lens injecting device having a slidable plunger with a damper to control the movement of the plunger and in effect control the release of the deformable intraocular lens into the eye.

- 9 -

A tenth object of the present invention is to provide a deformable intraocular lens injecting system comprising a lens injecting device having a slidable plunger with a spring and a damper to control the movement of the plunger and in effect control the release of the deformable intraocular lens into the eye.

5

An eleventh object of the present invention is providing a method of implantation of a deformable intraocular lens into the eye by forcing the deformable intraocular lens in a folded or condensed configuration through a passageway extending through an incision in the eye while applying an opposite force to control release of the deformable intraocular lens from the
10 passageway into the eye.

The present invention is directed to controllably releasing a folded or condensed deformable intraocular lens into the eye to reduce the risk of harm or damage to a patient's eye during the surgical procedure.

15

The present invention is directed to apparatus and methods of controlling the release of the advancing folded or condensed deformable intraocular lens by applying a force in a direction opposite to the direction of advancement of the deformable lens when being inserted into the eye. The force can be a constant or variable force, and the force can be selectively applied.
20 These different types of forces can be applied mechanically, fluidly, pneumatically,

- 10 -

magnetically, electrically, electromagnetically, combinations of forces, etc. However, mechanically means of applying the force by a spring and/or damper arrangement(s) provide for simple, inexpensive and reliable designs, and currently appear to be the most promising for future developments.

5

Various configurations of a spring or combination of springs can be applied in the present invention. For example, a coiled spring, cantilever spring, or spring arrangement utilizing the resilient property of the spring's structural configuration and/or the elastic property of the material forming the spring (e.g. plastic resin tubing, longitudinal slits in sides of harder plastic tubing providing a plurality of plate-like springs connected together at ends, plastic or rubber grommets or diaphragms).

10 The lens injecting device according to the present invention is preferably configured to apply an opposite force to the advancing plunger when the deformable intraocular lens is exiting the nozzle of the lens injecting device to provide controlled release of the deformable intraocular lens into the eye. In a preferred embodiment, the opposite force is applied to the advancing plunger only near the end of its stroke when the deformable intraocular lens is about to exit the tip of the nozzle. This arrangement allows the plunger to freely slide unimpeded most of the distance of its stroke yet provide sufficient back pressure at the end of its stroke to prevent 15 sudden plunger advancement as the intraocular lens exits the nozzle.

Brief Description of the Drawings

Fig. 1 is a side elevational view of a preferred embodiment of the lens injecting device according to the present invention.

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Fig. 2 is a top planar view of the lens injecting device shown in Fig. 1.

Fig. 3 is a side elevational view of the slidably disposed plunger disassembled from the lens injecting device shown in Fig. 1 to show its detailed structural configuration.

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Fig. 4 is a detailed cross-sectional view of an alternative embodiment of the thumb grip having a cylindrical recess to accommodate a fastener having a threaded bore.

15

Fig. 5 is a detailed broken away cross-sectional view showing the manner in which the sleeve stop mounted on the slidable plunger engages with an end face of the cylindrical barrel to engage the coiled spring causing a spring force opposite in direction to the advancing slidable plunger.

20

Fig. 6 is a detailed cross-sectional view as indicated in Fig. 1 of the cylindrical barrel and finger grip.

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Fig. 7 is a partial broken away view of an alternative spring made of resilient material, e.g. plastic, mounted on the slidable plunger.

5 Fig. 8 is a detailed longitudinal cross-sectional view of an alternative sleeve stop having a frictional lining to function as a damper to provide resistance of movement of the advancing slidable plunger.

10 Fig. 9 is a diagrammatic view of a slidable plunger provided with a spring for applying force in an opposite direction of advancement of the slidable plunger.

Fig. 10 is a diagrammatic view of a slidable plunger provided with a damper to function as a damper to provide resistance of movement of the advancing slidable plunger.

15 Fig. 11 is a diagrammatic view of a slidable plunger provided with both a spring and damper.

Fig. 12 is a perspective view of a prior art embodiment of a shooter device of STAAR Surgical Company of Monrovia, California.

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Fig. 13 is a longitudinal cross-sectional view of the prior art shooter device shown in Fig. 13.

Detailed Description of Preferred Embodiments

5

A preferred embodiment of a lens injecting device 10 as shown in Figures 1 and 2. This lens injecting device is configured for receiving a lens cartridge having a lens holding portion connected to a nozzle portion, and disclosed in the parent applications referred to in the section under related applications.

10

The lens injecting device 10 comprises a cylindrical barrel 12 having a lens cartridge receiver 14, and a slidable plunger 16 having a plunger tip 18. Further, the cylindrical barrel 12 is provided with a finger grip 20 and the slidable plunger 16 is provided with a thumb grip 22 for manipulating the lens injecting device 10.

15

In the preferred embodiment shown in Figures 1 and 2, a spring 24 is provided to create a force between the cylindrical barrel 12 and slidable plunger 16. Specifically, the coil type spring 24 is wrapped around a portion of the plunger 16, as indicated on the left-hand side of Figure 3. Further, the coil type spring 24 extends between the thumb grip 22 and the sleeve 20 stop 26. The face of fastener nut 30 and the end face 26a act as end stops for the spring 24

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causing the spring 24 to functionally engage with the slidable plunger 16 when the slidable plunger 16 is moved in a right-ward direction sufficiently to engage an opposite end face 26b of the sleeve stop 26 with the end face 12a of the cylindrical barrel 12, as shown in detail in Figure 5.

5

The thumb grip 22 is connected to one end of the slidable plunger 16. For example, the one end of the slidable plunger 16 can be provided with a threaded end portion 16a to be threaded into a threaded bore 22b of the thumb grip 22. In this embodiment of the thumb grip 22', the thumb grip 22' is provided with a cylindrical recess 28 for accommodating a fastener nut 30 threaded onto the end of threaded end portion 16a of the slidable plunger 16. This configuration allows the coil spring 24 to be positioned on the end portion of the slidable plunger 16 and locked in place by the fastener nut 30 prior to the threaded end portion 16a of the slidable plunger 16 being threaded into the threaded bore 22b of the thumb grip 22. This configuration facilitates assembly of the lens injecting device, and more securely restrains the coil spring 24 on the one end of the plunger 16.

The plunger 16 is provided with a lower groove 16b for receiving a inwardly extending protrusion 12b of the cylindrical barrel 12 to provide a locking key way arrangement to prevent relative rotation of the slidable plunger 16 within the cylindrical barrel 12 (i.e., maintains a fixed orientation of the slidable plunger 16 to prevent rotation within the cylindrical barrel 12).

Further, the finger grip 20 is securely connected to the cylindrical barrel 12 to prevent any relative movement there between. For example, the finger grip 20 is provided with a through bore that interference fits with the outer surface of a portion of the cylindrical barrel 12.

5 In an alternative embodiment as shown in Figure 7, the coil spring 24 is replaced with a section of resilient rubber or plastic tubing 24' performing the function of a spring due to the resilient nature of the material making up the section of tubing. As a further alternative, as shown in Figure 8, a sleeve stop 26' having a frictional lining 32 (e.g., synthetic plastic, ceramic, metal, glass, etc.) provides somewhat of a friction fit with an outer surface of the
10 plunger to function as a damper resisting the forward movement of the slidable plunger to control release of the deformable intraocular lens from the tip of the nozzle portion of the lens cartridge.

15 The examples of springs and dampers discussed above are only illustrative examples embodying the concepts of the present invention, however, other types of springs (e.g., cantilever type) and/or dampers (e.g., viscous fluid medium between plunger and cylindrical barrel) can be provided as alternatives to the preferred embodiment shown.

20 Figures 9 through 11 schematically illustrate applying a spring force, applying a damping resistance force, and combining both spring force and damping resistance force, respectively,

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for controlling the forward movement of the slidable plunger and for controlling the release of the deformable intraocular lens from the nozzle of the injecting device.

The method according to the present invention involves providing either a spring force,
5 or damping resistance force against a force for inserting the deformable intraocular lens through a passageway of a device for inserting a deformable intraocular lens through an incision in the eye. The spring force and/or damping resistance force control the forward advance of the deformable intraocular lens through the passageway for controlling the release thereof into the eye.

10

I Claim:

1. A deformable intraocular lens injecting device for inserting a deformable intraocular lens through a small incision in the eye, comprising:
 - 5 a sleeve having a lens receiver for accommodating a deformable intraocular lens;
 - a lens injecting nozzle disposed at one end of said sleeve, said nozzle including a passageway for directing the deformable intraocular lens to a nozzle tip;
 - a plunger slidably received within said sleeve, said plunger having a plunger tip for contacting the deformable intraocular lens at one end and a grip for actuating said plunger at an opposite end thereof;
 - 10 a spring associated with said plunger for providing a spring force against said plunger when said plunger tip is forcing the deformable intraocular lens from said nozzle tip to provide controlled release of the deformable intraocular lens from said nozzle tip.
- 15 2. A device according to Claim 1, wherein said spring is constantly engaging said plunger.
3. A device according to Claim 1, wherein said spring engages with said plunger when said plunger is reaching an end of a full length of its delivery stroke.

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4. A device according to Claim 3, wherein said spring engages said plunger when said plunger tip is located in said passageway through said nozzle.

5. A device according to Claim 1, wherein said spring provides sufficient spring force on said plunger to cause the plunger to rebound to some extent after said plunger reaches its full length delivery stroke.

6. A device according to Claim 5, wherein said spring provides a sufficient spring force to fully withdraw said plunger tip back inside said passageway through said nozzle.

10

7. A device according to Claim 1, including a damper associated with said plunger for resistance against the movement of said plunger when said plunger tip is forcing the deformable intraocular lens from said nozzle tip to provide controlled release of the deformable intraocular lens from said nozzle tip.

15

8. A device according to Claim 1, including a lens cartridge for containing the deformable intraocular lens,

wherein said lens receiver of said sleeve is a lens cartridge receiver for accommodating said lens cartridge containing said deformable intraocular lens, and said nozzle is defined by a
20 nozzle portion connected to a lens holding portion of said lens cartridge.

9. A deformable intraocular lens injecting device for inserting a deformable intraocular lens through a small incision in the eye, comprising:
 - a sleeve having a lens receiver for accommodating a deformable intraocular lens;
 - 5 a lens injecting nozzle disposed at one end of said sleeve, said nozzle including a passageway for directing the deformable intraocular lens to a nozzle tip;
 - a plunger slidably received within said sleeve, said plunger having a plunger tip for contacting the deformable intraocular lens at one end and a grip for actuating said plunger at an opposite end thereof;
- 10 a damper associated with said plunger for providing a resistance against movement of said plunger when said plunger tip is forcing the deformable intraocular lens from said nozzle tip to provide controlled release of the deformable intraocular lens from said nozzle tip.
- 15 10. A device according to Claim 9, wherein said damper is constantly engaging said plunger.
11. A device according to Claim 9, wherein said damper engages with said plunger when said plunger is reaching an end of the full length of its delivery stroke.
12. A device according to Claim 11, wherein said spring engages said plunger when said plunger tip is located in said passageway through said nozzle.

- 20 -

13. A device according to Claim 9, wherein said spring provides sufficient spring force on said plunger to cause the plunger to rebound to some extent after said plunger reaches its full length delivery stroke.

5

14. A device according to Claim 13, wherein said spring provides a sufficient spring force to fully withdraw said plunger tip back inside said passageway through said nozzle.

15. A device according to Claim 9, including a spring associated with said plunger for providing a spring force against said plunger when said plunger tip is forcing the deformable intraocular lens from said nozzle tip to provide controlled release of the deformable intraocular lens from said nozzle tip.

16. A device according to Claim 9, including a lens cartridge for containing the deformable intraocular lens,

wherein said lens receiver of said sleeve is a lens cartridge receiver for accommodating said lens cartridge containing the deformable intraocular lens, and said nozzle is defined by a nozzle portion connected to a lens holding portion of said lens cartridge.

17. A deformable intraocular lens injecting system for inserting a deformable intraocular lens through a small incision in the eye, comprising:

a lens cartridge for containing the deformable intraocular lens, said lens cartridge comprising a lens holding portion connected to a nozzle portion;

5 a sleeve having a lens cartridge receiver for accommodating said lens cartridge with said nozzle portion extending from one end of said sleeve, said nozzle portion including a passageway for directing the deformable intraocular lens to a nozzle tip;

10 a plunger slidably received within said sleeve, said plunger having a plunger tip for contacting the deformable intraocular lens at one end and a grip for actuating said plunger at an opposite end thereof;

a resistance device associated with said plunger for providing a resistance against movement of said plunger when said plunger tip is forcing the deformable intraocular lens from said nozzle tip to provide controlled release of the deformable intraocular lens from said nozzle tip.

15

18. A device according to Claim 17, wherein said resistance device is a spring.

19. A device according to Claim 17, wherein said resistance device is a damper.

20. A device according to Claim 17, wherein said resistance device includes both a spring and a damper.

21. A method of inserting a deformable intraocular lens through a small incision in the eye, comprising the steps of:

loading the deformable intraocular lens into a lens injecting device having a passageway extending through the incision in the eye; and

forcing the deformable intraocular lens through the passageway against a resistance of the force applied to control release of the deformable intraocular lens from an exit end of the passageway inside the eye.

22. The method of Claim 21, wherein the resistance is a constant resistance.

23. The method of Claim 21, wherein the resistance is a variable resistance.

15 24. The method of Claim 23, wherein the resistance increases in the direction of movement of the deformable intraocular lens into the eye.

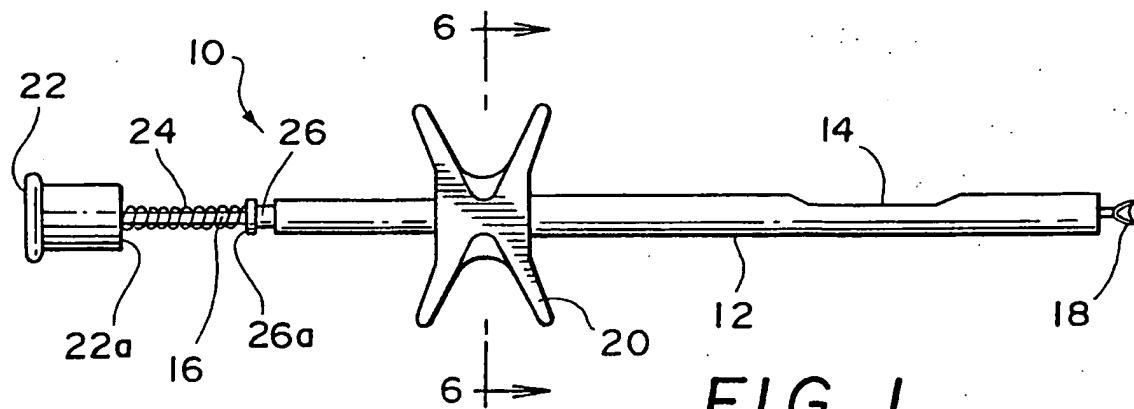


FIG. 1

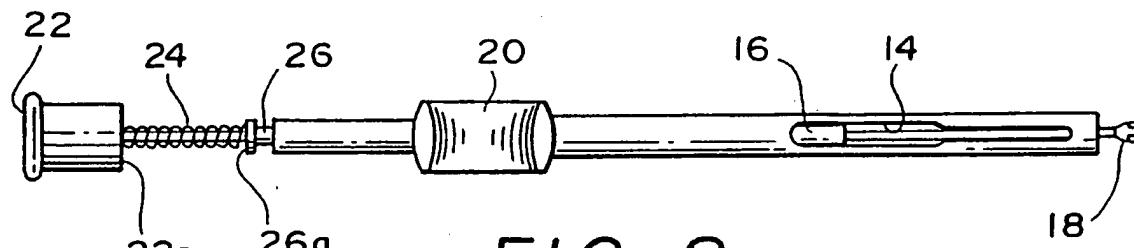


FIG. 2

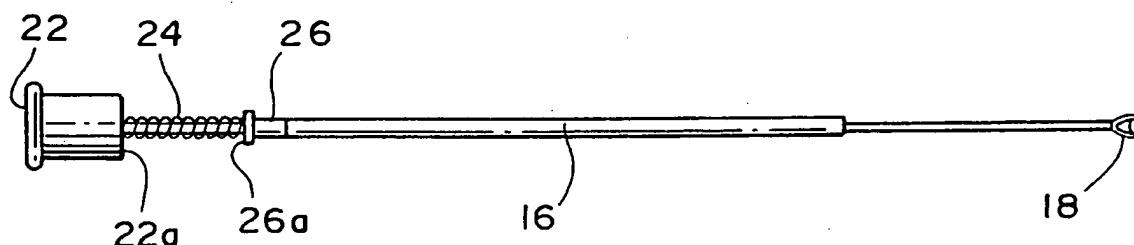


FIG. 3

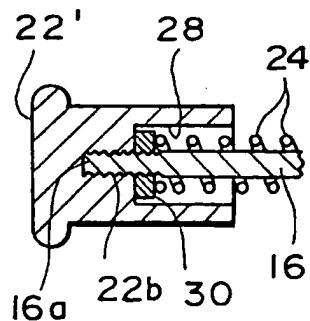


FIG. 4

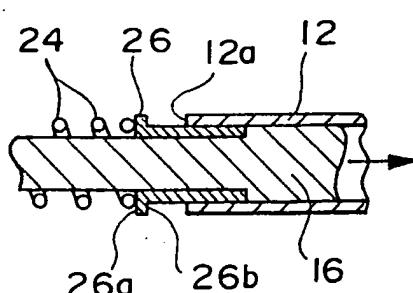


FIG. 5

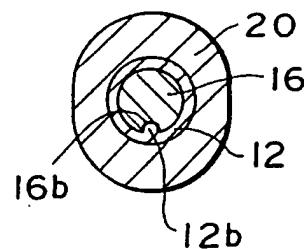


FIG. 6

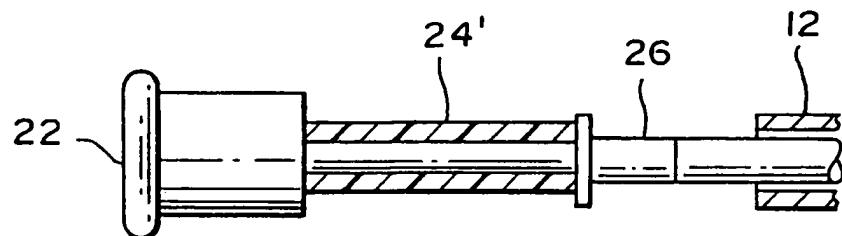


FIG. 7

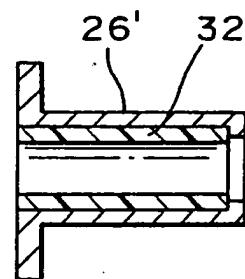


FIG. 8

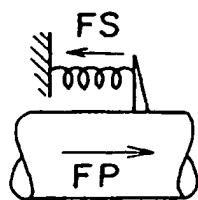


FIG. 9

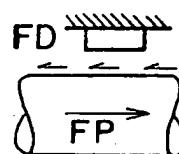


FIG. 10

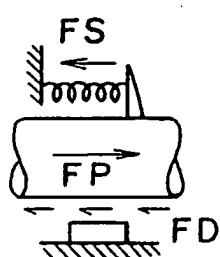


FIG. 11

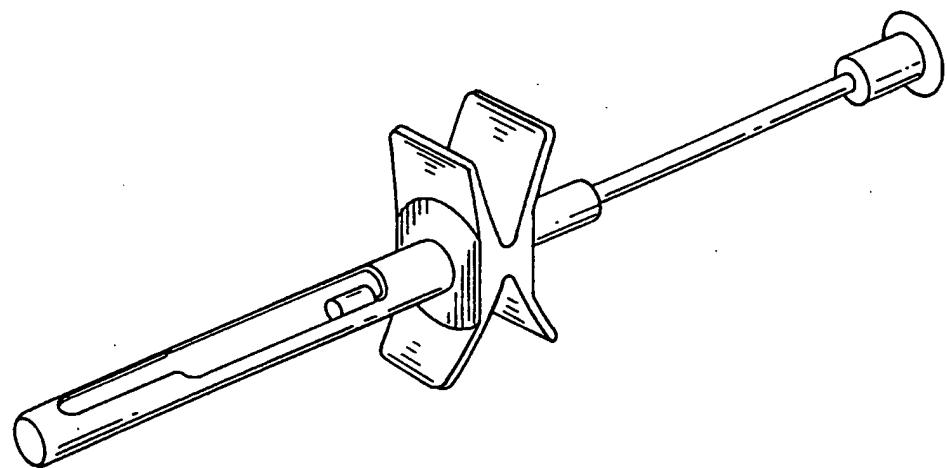


FIG. 12
(PRIOR ART)

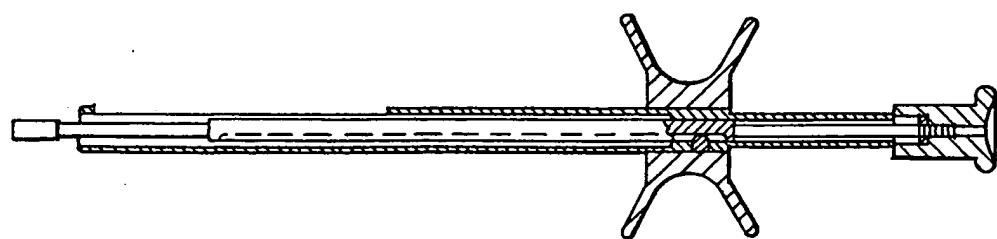
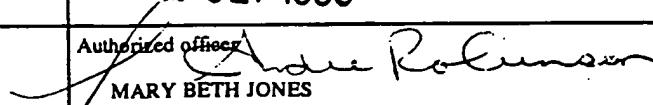


FIG. 13
(PRIOR ART)

INTERNATIONAL SEARCH REPORT

International application No.
PCT/US96/07750

A. CLASSIFICATION OF SUBJECT MATTER		
IPC(6) : A61B 17/00 US CL : 606/107 According to International Patent Classification (IPC) or to both national classification and IPC		
B. FIELDS SEARCHED		
Minimum documentation searched (classification system followed by classification symbols) U.S. : 604/57-64; 606/107; 623/6		
Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched		
Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)		
C. DOCUMENTS CONSIDERED TO BE RELEVANT		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US, A, 4,597,753 (TURLEY) 01 July 1986, see column 4 line 6 to column 5 line 8, and column 5 lines 34-63,	1-20 -----

Y		21-24
Y	US, A, 5,304,182 (RHEINISH ET AL.) 19 April 1994, see column 2 line 32 to column 3 line 15.	21-24
<input type="checkbox"/> Further documents are listed in the continuation of Box C. <input type="checkbox"/> See patent family annex.		
* Special categories of cited documents: "A" document defining the general state of the art which is not considered to be part of particular relevance "E" earlier document published on or after the international filing date "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified) "O" document referring to an oral disclosure, use, exhibition or other means "P" document published prior to the international filing date but later than the priority date claimed		
Date of the actual completion of the international search 11 SEPTEMBER 1996		Date of mailing of the international search report 26 SEP 1996
Name and mailing address of the ISA/US Commissioner of Patents and Trademarks Box PCT Washington, D.C. 20231 Facsimile No. (703) 305-3590		Authorized officer  MARY BETH JONES Telephone No. (703) 308-3400

INTERNATIONAL SEARCH REPORT

International application No.
PCT/US96/07750

Box I Observations where certain claims were found unsearchable (Continuation of item 1 of first sheet)

This international report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. Claims Nos.:
because they relate to subject matter not required to be searched by this Authority, namely:

2. Claims Nos.:
because they relate to parts of the international application that do not comply with the prescribed requirements to such an extent that no meaningful international search can be carried out, specifically:

3. Claims Nos.:
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

Box II Observations where unity of invention is lacking (Continuation of item 2 of first sheet)

This International Searching Authority found multiple inventions in this international application, as follows:

Please See Extra Sheet.

1. As all required additional search fees were timely paid by the applicant, this international search report covers all searchable claims.
2. As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment of any additional fee.
3. As only some of the required additional search fees were timely paid by the applicant, this international search report covers only those claims for which fees were paid, specifically claims Nos.:

4. No required additional search fees were timely paid by the applicant. Consequently, this international search report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

Remark on Protest

The additional search fees were accompanied by the applicant's protest.
 No protest accompanied the payment of additional search fees.

INTERNATIONAL SEARCH REPORT

International application No.
PCT/US96/07750

BOX II. OBSERVATIONS WHERE UNITY OF INVENTION WAS LACKING

This ISA found multiple inventions as follows:

Claims 1-20, Group I, directed to an article for insertion capable of use with a deformable intraocular lens.

Claims 21-24, Group II, directed to a method of using a deformable intraocular lens and an insertion device.

Groups I and II, the inventions listed in these groups do not relate to a single inventive concept under PCT Rule 13.1 because, under PCT Rule 13.2, they lack the same or corresponding special technical features for the following reasons:

Group I requires a particular inserter not required for Group II.

Group II requires the use of a deformable intraocular lens, which lens is not required in Group I.